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Gender Differences in Lower Limb Frontal Plane Kinematics During Landing

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Abstract.

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The study aimed to investigate gender differences in knee valgus angle and interknee and inter-ankle distances in university volleyball players when performing opposed block jump landings. Six female and six male university volleyball players performed three dynamic trials each where subjects were instructed to jump up and block a volleyball suspended above a net set at the height of a standard volleyball net as it was spiked against them by an opposing player. Knee valgus/varus, interknee distance and inter-ankle distance (absolute and relative to height) were determined during landing using 3D motion analysis. Females displayed significantly greater maximum valgus angle and range of motion than males. This may increase the risk of ligament strain in females compared with males. Minimum absolute interknee distance was significantly smaller in females and absolute and relative interknee displacement during landing was significantly greater in females compared with males. Both absolute and relative inter-ankle displacement during landing was significantly greater in males than females. These findings suggest that the gender difference in the valgus angle of the knee during two-footed landing is influenced by gender differences in the linear movement of the ankles as well as the knees. Coaches should therefore develop training programmes to focus on movement of both the knee and ankle joints in the frontal plane in order to reduce the knee valgus angle during landing which in turn may reduce the risk of non-contact ACL injury.

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Introduction.

Anterior Cruciate ligament (ACL) injury is a common injury and approximately 70% these injuries occur in sport (Faegin, 1988; Johnson, 1988; Smith *et al.*, 1988). ACL rupture is a debilitating injury and can cause long-term absence from participation in a sport and, in some cases, enforced retirement. Between 70% and 90% of ACL injuries have been reported to be non-contact in nature, i.e., no direct contact with the knee at the time of injury (Woodland and Francis, 1992; McNair *et al.*, 1993; Mykelbust *et al.*, 1997; Griffin *et al.*, 2000). The incidence on non-contact ACL injury in females has been reported to be 6 to 8 times greater than in males competing in the same sports (Chandy and Grana, 1985; Gray *et al.*, 1985; Ferretti *et al.*, 1992; Paulos, 1992; Malone *et al.*, 1993; Lidenfeld *et al.*, 1994; Arendt and Dick, 1995; Gwinn *et al.*, 2000).

Non-contact ACL injuries appear to be common in activities involving landing (Hume and Steele; 1997, Otago and Neal; 1997), deceleration (Miller *et al.*, 1995) and rapid change of direction (Bartold, 1997). The incidence of ACL injury is therefore relatively high in sports such as basketball, netball, handball and volleyball that are characterised by a high frequency of landing, decelerating and rapid changes of direction (Arendt and Dick, 1995; Griffin *et al.*, 2000).

Whilst the muscle moments about the joints of the lower limbs largely determine the movement patterns of the lower limbs, the resulting angular kinematics may provide some indication of the strain on the joint ligaments. The greater the range of

abnormal joint movement (movement outside a joint's normal range of motion), the greater the possibility of strain on associated ligaments (Watkins, 1999). ACL injury is often associated with valgus movement of the knee at the time of injury (Boden *et al.*, 2000; Olsen *et al.*, 2004). For example, Olsen *et al.* (2004) analysed videotapes of game situations in which ACL injury occurred in team handball in order to identify the mechanisms for ACL injury. Three physicians were used to identify factors relating to the knee position such as estimated varus-valgus angle. The results showed that the knee was in a valgus position in all of the 20 cases analysed and the estimated valgus angle was above 10° in 19 of the 20 cases. Therefore it was concluded that valgus knee movement is a high risk factor for ACL injury.

Since increased valgus angle during dynamic movement has been associated with an increased likelihood of ACL injury a number of studies have investigated the frontal plane kinematics of the knee during landing/cutting. These studies report that females tend to exhibit greater maximum knee valgus angle and greater range of motion (from initial contact to maximum) when landing/cutting than males (Malinzak et al., 2001; Ford et al., 2003; Kernozek et al., 2005). Consequently, the reported greater maximum knee valgus angle in females when landing may increase the risk of ACL injury relative to males. However, the valgus angle of the knee is related to the linear movement of the knee and ankle joints. At present there is little knowledge of the relative contribution of the linear movements of the knee and ankle joints to the reported greater valgus angle in females compared with males during landing. During a two-footed landing manoeuvre, the distances between corresponding joints in the right and left leg, i.e., distance between right and left knees, (inter-joint distances) may provide more insight into the influence of the linear movements of the knee and

ankle joints on the increased valgus angle of the knee in females than looking at the knee joint in isolation.

Aim.

The aim of the study was to investigate the effects of gender on knee valgus angle and inter-knee and inter-ankle distances in university volleyball players performing block jump landings.

Methods.

Subjects.

Data were obtained for six male (Mean age 21.6 ± 3.3 years, mass 70.1 ± 3.1 kg and height 175.7 ± 8.6 cm) and six female (Mean age 21.2 ± 1.3 years, mass 57.6 ± 7.5 kg and height 164.8 ± 7.5 cm) university volleyball players. All subjects were right leg dominant and had no previous history of hip/knee or ankle injury. Written consent forms approved by the departmental ethics committee were signed by all subjects prior to data collection.

Measurement system.

Two adjacent AMTI force platforms embedded into the laboratory floor sampling at 600 Hz were used to measure ground reaction force to determine initial ground contact of right and left legs on landing. A 12 camera Vicon 512 system (Vicon, Oxford, England) sampling at 120 Hz was used to determine 3D coordinates of 16 retro-reflective markers (25 mm diameter). Markers were placed directly on the skin

over anatomical landmarks in accordance with the Vicon system's lower body plug-in gait marker set; right and left anterior superior iliac spines, right and left posterior superior iliac spines, lower lateral surface of the right and left thigh along the line between the hip and knee joint markers, right and left lateral epicondyle the femur, lower lateral surface of the right and left tibia along the line between knee and ankle joint markers, right and left lateral malleolus, superior proximal end of the second metatarsal of the right and left foot, posterior aspect of the Achilles tendon of the left and right leg at the same height as the second metatarsal marker. From the location of the markers placed on the body, combined with required anthropometric measurements (height, weight, leg length, knee width and ankle width) of each subject, the Vicon system calculated the 3D coordinates of hip, knee and ankle joint centres which were used to determine the thigh and shank segment local reference planes. In the plug-in gait system, the measurement of knee valgus/varus angle was determined as the Euler angle of the shank segment reference frame relative to the thigh segment reference plane rotated in the order 1) flexion/extension, 2) valgus/varus, 3) internal/external rotation. The valgus/varus angle is the angle between the distal extension of the thigh axis and the shank axis. A positive angle indicates varus and a negative angle indicates valgus (Figure 1). Inter-joint distances were calculated as the linear distance in 3D between the corresponding lower limb joint centres of the right and left leg (i.e., distance between right and left knee joint centres) for the knee and ankle joints. Based on a frequency content analysis of the 3D coordinate data, marker trajectories were filtered using a Woltring Filter with a low-pass cut-off frequency of 10 Hz and stop-band frequency of 30 Hz.

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Figure 1 about here.

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Testing procedure.

The laboratory was set up with a rope fixed horizontally to act as a volleyball net at a height of 2.43 m for male subjects and 2.24 m for female subjects (height of a standard volleyball net). The net was placed 5 cm in front of and parallel to the adjacent force platforms. In addition to the net, a volleyball was suspended from the ceiling so that it was positioned 5 cm above the height of the net (2.48 m for males and 2.29 m for females) and with the centre of the ball 10 cm in front of the line of the net (the other side of the net to where the subject (blocker) was standing). The ball was positioned vertically above the line separating the two force platforms. The jumping and landing task was made as realistic as possible by having subjects attempt to block an actual spike performed by an experienced volleyball player. At the start of each trial, the subject stood with each foot on a separate force plate. The subject then timed his/her blocking action in order to try to block the ball as it was spiked. The ball was spiked from the same suspended position in order to eliminate variation in the position and velocity of the ball. On landing, each foot landed on a separate force plate. Following appropriate warm up and practice, data was recorded for three successful trials for each subject.

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Data analysis.

The angular displacement of the knee (mean data for right and left legs combined) in the frontal (valgus/varus) plane along with the inter-knee and inter-ankle distances were determined between initial ground contact and the end of landing, which was defined as, depending on which occurred later in each trial, either maximum knee flexion or maximum knee valgus angle. Time – series data were then normalised with respect to average trial time. Inter-joint distances were also normalised to height to account for gender differences in body size (expressed as percentage height, %ht). Independent-samples t-tests were carried out on the angular displacement and interjoint data at initial ground contact, maximum and/or minimum values and range of motion to examine gender differences. Due to multiple t-tests (15) being carried out on samples taken from the same population, to reduce the chance of type I error, a Bonferroni adjustment was made to the alpha level.

Results.

Knee valgus/varus angle.

Figure 2 shows females contacted the ground in a slight valgus position (–ve values) which progressively increased between initial ground contact and the end of landing. Males, however, contacted the ground in a slight valgus position and moved into a slight varus position (+ve values) at the end of landing (Table 1 and Figure 2). The valgus angle at initial ground contact was not significantly different between males and females. However, the range of motion and the maximum valgus angle were significantly greater in females compared with males (Table 1 and Figure 2).

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 Table 1 about here.
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Figure 2 about here.
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Inter knee and inter ankle displacements.

There was no significant difference in absolute or relative inter-knee distance at initial ground contact between males and females. The absolute minimum inter-knee distance was significantly longer for males than females but there was no significant difference in the relative minimum inter-knee distance between males and females. The change in both absolute and relative inter-knee distance between initial ground contact and the end of landing was significantly smaller for males than females. There was no significant difference between males and females in absolute or relative inter-ankle distance at ground contact or minimum distance. However, the change in absolute and relative inter-ankle distance between initial ground contact and the end of landing was significantly greater in males than females (Table 1 and Figures 3 and 4).

Figure 3 about here.

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215 Figure 4 about here. 217

Discussion and Implications.

Knee valgus/varus angle.

The results show that females exhibited significantly greater maximum knee valgus angle and significantly greater range of motion of knee valgus angle than males

(Table 1 and Figure 2). This finding is supported by a number of previous studies (Malinzak *et al.*, 2001; Ford *et al.*, 2003; Kernozek *et al.*, 2005). However, the values reported in this study are different to previous results, particularly for females. For example, Kernozek *et al.* (2005) reported values of $0.7 \pm 6.9^{\circ}$ for males and $-24.9 \pm 8.5^{\circ}$ for females for maximum knee valgus angle (valgus -ve / varus + ve), compared with $0.6^{\circ} \pm 9.1$ for males and $-10.4^{\circ} \pm 7.7$ for females in this study. There are a number of possible reasons for these differences which include subjects' playing standard and task demands. For example, in Kernozek *et al.* (2005) the subjects used were recreational athletes whereas university athletes were used in this study. Also, the effect of opposition in the present study may have resulted in differing levels of conscious control over the landing manoeuvre than in the Kernozek *et al.* (2005) study which involved an unopposed drop landing task.

Since increased knee valgus angle during landing has been associated with increased risk of ACL injury (Boden *et al.*, 2000; Olsen *et al.*, 2004), the increased knee valgus angle exhibited by females compared with males during landing in the present study may suggest an increased risk of ACL injury in females compared with males. This in turn may be associated with the increased incidence of non-contact ACL injury in females compared with males.

Inter knee and inter ankle displacements.

The results of the inter-knee distances indicate that females' knees move significantly closer together and move through a greater absolute and relative distance during landing than males (Table 1), which is also reported by Ford *et al.* (2003). In the Ford

et al. (2003) study, inter-knee distance was measured from markers placed on the lateral epicondyles of each femur, whereas in this study inter-knee distance was measured from estimated knee joint centres. Each estimated knee joint centre incorporates an offset equivalent to the sum of half the knee width and the marker radius. The knee joint centre is located as the offset from the marker located on the lateral epicondyle the femur in a direction perpendicular to the line from the hip joint centre to lateral epicondyle the femur marker. To compare the data from this study with that of Ford et al. (2003) the average knee offsets of 122.1 mm for males and 117.2 mm for females were applied to the Ford et al. (2003) data. The amended Ford et al. (2003) data for minimum inter-knee distance (males: 223.9 mm \pm 6; females 203.8 mm \pm 6) is similar to the results of the present study (males: 233.7 mm \pm 39.4; females: 200.0 mm \pm 34.5). However, the amended Ford et al. (2003) data for inter-knee displacement during landing (males: 53 mm \pm 5; females: 73 mm \pm 5) indicate greater displacement compared with the present results (males: 10.2 mm \pm 16.5; females: 27.9 mm \pm 18.0).

To our knowledge, no data has been reported for inter-ankle distances during two-footed landing manoeuvres. Therefore no comparisons can be made between the results of this study and previous studies. The inter-ankle results indicate that, after initial ground contact, the ankle joint linear motion was greater in males than females in both absolute and relative terms. From Table 1 and Figures 3 and 4 it can be seen that males' ankles are wider apart at initial ground contact and move together more quickly than in females for the first 40% of normalised contact time. Thereafter, the inter-ankle distance is similar in males and females. This is likely to be because the heels are in contact with the ground during this period. The movement patterns

indicate that after the toes make contact with the ground, females' ankles move vertically downward to the ground until the heels make contact, whereas for males, the ankles are brought in towards each other as the heels move down to the ground. When looking at the simultaneous linear motion of the knees and ankles on landing (Figures 3 and 4), a continuous inward movement of the ankles is shown by males and females, however, this inward movement of the ankles is greater in males than females. At the same time, the movement of the knees in males show an out – in – out action resulting in minimum net movement. In contrast, the females' knees show continuous inward movement.

Conclusions.

During two-footed landing females exhibited significantly greater maximum valgus angle and range of motion of knee valgus angle than males. Furthermore, the absolute and relative inter-knee displacement during landing was significantly greater in females than males, whereas absolute and relative inter-ankle displacement during landing was significantly smaller in females than males. These results indicate that the greater knee valgus angle exhibited by females during landing may be influenced by gender differences in the combined linear movements of the knee and ankle joints rather than the knees in isolation. This greater knee valgus angle in females may increase the risk of ligament strain in females relative to males which may contribute to the gender difference in the incidence of non-contact ACL injury. Coaches should therefore incorporate exercises into training programmes to reduce the knee valgus angle in females during two-footed landing. Furthermore, these exercises should

- focus on the movement of the ankles as well as the knees in reducing knee valgus during landing.

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		Male	s	Females		
	-	Absolute	Relative	Absolute	Relative	
	IC	-2.8 ± 5.9	NA	-1.6 ± 2.8	NA	
Valg/var	MAX_{VAL}	-2.9 ± 7.9*	NA	-10.4 ± 7.7*	NA	
(°)	MAX_{VAR}	0.6 ± 9.1	NA	N/A	NA	
	ROM	3.5 ± 9.6*	NA	8.8 ± 7.8*	NA	
Inter-knee	IC	244.0 ± 33.0	13.9 ± 1.9	227.9 ± 29.4	13.8 ± 1.8	
distance	MIN	233.7 ± 39.4*	13.3 ± 2.2	200.0 ± 34.5*	12.1 ± 2.1	
(mm / %ht)	ROM	10.2 ± 16.5*	0.6 ± 0.9*	27.9 ± 18.0*	1.7 ± 1.1*	
Inter-ankle	IC	310.6 ± 58.4	17.7 ± 3.3	288.6 ± 46.3	17.5 ± 2.8	
distance	MIN	269.0 ± 58.7	15.3 ± 0.9	264.8 ± 45.8	16.1 ± 2.8	
(mm / %ht)	ROM	41.6 ± 27.4*	2.4 ± 1.6*	23.7 ± 16.5*	1.4 ± 1.0*	

^{*:} Significant difference between males and females (p < 0.01).